

RESEARCH ARTICLE

Comparison of Double and Single Leg Weight-Bearing Radiography in Determining Knee Alignment

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Abstract

Background: Knee malalignment is an important modifiable cause of osteoarthritis (OA). Surgical therapeutic procedures depend on proper knee alignment assessment. The purpose of this study was to compare knee alignment parameters between double and single leg weight-bearing radiographs and to evaluate the reproducibility of inter- and intra-observer measurements.

Methods: One hundred eight patients (59 male and 49 female) with knee deformity visited at Kerman Knee Clinic were selected. Full limb anteroposterior (AP) Radiographs were taken for each participant in double and single leg weight-bearing positions. Hip-Knee-Ankle Angle (HKAA), Medial-Proximal-Tibial Angle (MPTA), Lateral-Distal-Femoral Angle (LDFA) and Joint-Line-Convergence Angle (JLCA) measured. Images stored on PC were examined by three observers to assess inter and intra observer reproducibility. Data analysis was done by SPSS software.

Results: The mean age of patients was 48.4 (± 6.84) years, mean BMI was 26.55 (± 1.94) Kg/m². The mean HKAA and JLCA were significantly different between double and single leg weight-bearing radiographs. Intraclass correlation coefficient (ICC) test showed high (0.99) inter-reproducibility between three observers in all cases, except one (ICC=0.92). Intra-observer reproducibility indicated a strong correlation between the observer's measurements at different times (ICC > 0.99).

Conclusion: HKAA and JLCA were affected by the patient's position. Observer and time interval had no effect on either of HKAA, MPTA, LDFA, and JLCA. Also the measurement of knee alignment parameters was not dependent on observer's experience. In conclusion single leg weight-bearing radiography is more representative of knee alignment and is inter and intra-observer reproducible.

Keywords: Knee Alignment, Osteoarthritis, Radiography, Reliability

Introduction

Osteoarthritis (OA) as one of five leading causes of disability among non-institutionalized adults, affects more than 20 million individuals in the United States (1, 2). Varus and valgus alignment of the lower limb accelerate degenerative changes and knee OA progression (3-8). Knee malalignment can be modified surgically (9, 10) but a meticulous analysis of the deformity has to be achieved in order to define the type, size and site of deformity for optimized therapeutic planning, surgical technique, and postoperative follow-up (11). Radiographic examination, as a clinical assessment, is a fundamental tool for pre- and post-operative planning (12, 13).

The frontal plane alignment measures are the gold

standard method to assess knee alignment in patients with OA. Usual clinical tool for this purpose is full limb anteroposterior (AP) radiograph of lower extremities while the patient is standing on both feet (7, 13, 14).

Several different parameters measured in knee radiographs. One of the most common used parameters is the load-bearing axis (mechanical axis of the lower extremity), a line drawn from center of femoral head to center of the ankle. The orientation of this axis reflects alignment in standing position, since in a varus knee the line passes medial to the knee and in a valgus knee, the load-bearing axis passes lateral to the knee (12, 15).

Lower limb alignment depends on two geometry: the

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long bones and articulating surfaces of femur and tibia (16). Hip-Knee-Ankle Angle (HKAA) as the most common parameter that is measured by radiographs indicates the size of deformity. It is the angle formed by the intersection of a line from the center of femoral head to the center of the tibial spine and a second line from the center of talus to the center of the tibial spine. The normal HKAA is 180°, the angle greater than 180° represent a valgus deformity, and less than 180° a varus deformity (17, 18).

Medial Proximal Tibial Angle (MPTA), Lateral Distal Femoral Angle (LDFA) and Joint Line Convergence Angle (JLCA) determine alignment between tibial and femoral surfaces in weight-bearing position (12, 16). These angles are defined as follow; MPTA: The angle between the tibial mechanical axis and tibial joint line (line across the medial and lateral tibial plateaus) that is normally 87°. LDFA: The angle between the femoral mechanical axis and femoral joint line (line across the distal femoral condyles) that is normally 93°. JLCA: The angle between femoral and tibial joint line that is normally 0° - 2°, meaning they are almost parallel. Abnormal angle is due to asymmetric wear (12, 19-21).

The initiation of knee OA may be due to the femoral shaft curvature changes along with aging. The varus femoral condylar orientation, medial joint space narrowing, and tibial plateau compression are the secondary sign of OA progression (22).

During the stance phase of gait which encompasses sixty percent of the gait cycle, body weight supported by single leg (23). The mechanical axis angle is different in single-leg standing, double-leg standing, and supine positions (24).

In previous studies, lower limb axes and angles are drawn and measured on an AP radiograph which is taken while the patient is standing on both feet (3, 13, 22, 25, 26). Except for one study that compared and evaluated the reliability of mechanical axis between double and single leg weight-bearing (24), but other lower extremity alignment parameters have not been compared in weight bearing positions.

We designed this study to compare all four knee alignment parameters between double and single leg weight-bearing radiographs; and also to evaluate the reproducibility of inter- and intra-observer measurements.

Materials and Methods

Subjects

One hundred eight patients who had been visited at Kerman Knee Clinic, Kerman, Iran for knee deformity during Sep. 2012 to Oct. 2014 were selected. This study was approved by Kerman University of Medical Sciences Faculty of Medicine and the Committee of Ethics.

Anteroposterior (AP) full-limb radiograph (or Hip Knee Ankle) as the gold standard imaging modality for assessing lower limb alignment was used to determine knee deformity (varus or valgus) in patients who were clinically suspicious of knee malalignment (7). All the participants who attended in our study either had knee OA or were at high risk for developing knee OA. High risk individuals include who were overweight or obese, those with current knee pain and those with a history of knee

injury or surgery. Exclusion criteria were rheumatoid arthritis, ankylosing spondylitis, psoriatic arthritis, Reiter's syndrome, significant kidney disease, cancer, bilateral knee replacements, history of fracture, surgical treatment of OA (27). Eligible patients participated only if they gave the written informed consent to take another radiograph.

Radiographs

Antero-posterior full-limb radiographs in double leg weight-bearing position were taken with 130×36-cm graduated grid cassette to include the full limb of tall participants. The patients stood without footwear while their knees in full extension and tibial tubercles facing forward. The x-ray beam was centered at the knee with a setting of 100 to 300 mA/s and 80-90 kV, depending on limb size and tissue characteristics from 2.4m distance (7, 18).

Another radiograph was taken separately for each patient with above characteristic in a single leg weight-bearing position in which the patient raises one leg to put the weight completely on the malaligned knee.

Measurements

The digitalized images stored on a PC to be analyzed further using the software Medview Meddiag-©MEDECOM – 3.0.4. This digital software provides minimal bios in placing points and drawing lines.

The following four parameters were determined on both radiographs for each patient. 1. HKA angle (HKAA) which was the angle between the femoral mechanical axis (a line from the center of the femoral head running distally to the mid-condylar point) and tibial mechanical axis (line from the center of the tibial plateau extending distally to the center of the tibial plafond). 2. MPTA was the angle between the tibial mechanical axis and tibial joint line. 3. LDFA was the angle between the mechanical femoral axis and femoral joint line. 4. JLCA was the angle between distal femoral joint line and proximal tibial joint line (7, 12).

We used Medview Meddiag software to measure the above-mentioned angles as follow:

- The Observer put three points at femoral head borders and the software defined the circumscribed circle and the center of femoral head [Figure 1].

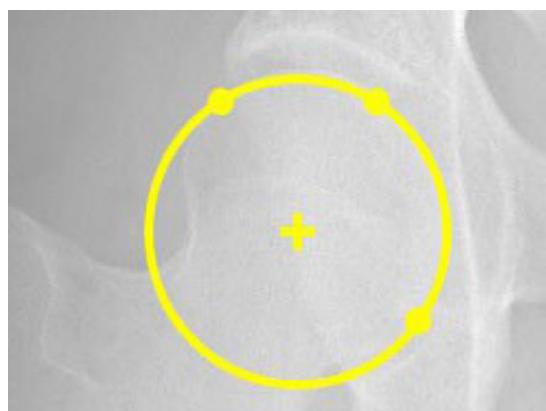


Figure 1. Defined the center of the femoral head.

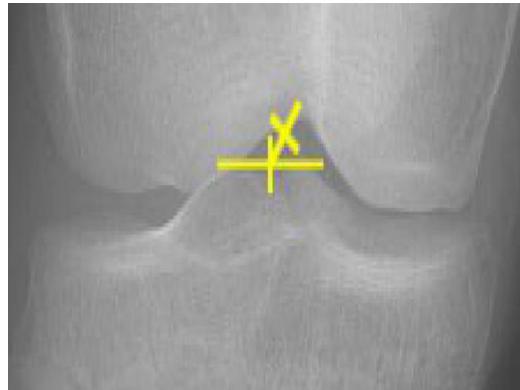


Figure 2. Intercondylar eminence of the tibia and Femoral intercondylar notch.



Figure 3. Inter malleolar segment tangent.

- The observer pointed femoral inter condylar notch and outlined inter condylar tibial eminence [Figure 2].
- After drawing inter malleolar line by observer [Figure 3], the software illustrated HKAA [Figure 4]



Figure 4. The tangent to the femoral condyles.

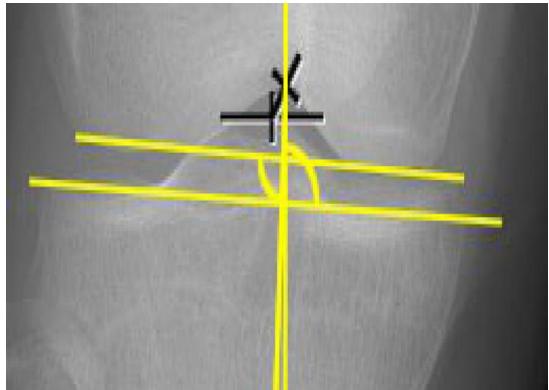


Figure 5. The tangent to the tibial plateau.



Figure 6. HKAA: Hip Knee Ankle Angle, MPTA: Medial Proximal Tibial Angle, LDFA: Lateral Distal Femoral Angle, JLCA: Joint Line Convergence measured and displayed on digital image.

- The Observer drew the tangent of femoral condyles and tibial plateau [Figure 4; 5] and the software outlined and measured all of the HKAA, MPTA, LDFA and JLCA on digital image [Figure 6]
- The reproducibility of this technique, was estimated by three distinct observers (an orthopedic surgeon with

sixteen years of experience and two medical students trained in epidemiology and knee alignment). To assess inter-observer reproducibility, each radiograph measurement (single and double leg) was done by all three observers in a blind circumstance with no knowledge of prior results. Intra-observer reproducibility was evaluated in two independent measurements accomplished by the orthopedic surgeon for each patient within two weeks.

Statistical analysis

To evaluate changes in double and single leg standing angles, Paired t-test was used. The intra- and inter-observer reproducibility was assessed by means of intraclass correlation coefficient (ICC) (28). As explained before, each participant was measured 2 times by 3 observers and in 2 positions (12 observations per subjects). Taking into account the dependency of observations, linear mixed effects regression analysis was used to evaluate the effect of positions, observers, and time on measurements. The SPSS program statistical software was used for analysis. A *P-value* of less than 0.05 was considered to be statistically significant.

Results

One hundred and eight patients (59 male and 49 Female) were selected for this study. Their mean age was 48.4 (± 6.84) years (range 31-60 years), mean body mass index (BMI) was 26.55 (± 1.94) Kg/m². Varus deformity was seen in 90.7% of patients.

According to Table 1, HKAA and JLCA were significantly different between double and single leg weight-bearing positions.

ICC test showed high inter-observer reproducibility between three observers in all angles. ICC was higher than 0.99 except for one (ICC=0.92). Intra-observer reproducibility demonstrated a strong correlation between the observer's measurements at different times (ICC > 0.99).

We have seen that observer had no effect on any of four

outcomes [Table 2]. For example, in terms of HKAA, the maximum difference seen between observers was as low as 8.37 and 8.49 which was far from being significant.

Table 2 illustrated that the time interval had no effect on the accuracy of evaluation of observer's measurements. The maximum difference of angle measurements was 0.05 between first and second time [Table 2].

Using linear regression [Table 2] determined that HKAA and JLCA were different between double and single weight-bearing positions.

Discussion

The purpose of this study was to compare knee alignment parameters between double leg and single leg weight-bearing radiographs and to evaluate the reproducibility of inter- and intra-observer measurements.

Our demographic results revealed that the majority of our patients with knee alignment have high body mass index which was predictable. Gudbergson et al. concluded that weight loss is effective for symptomatic relief in obese subjects with knee osteoarthritis (29). In the current study, the mean age of participants was above forty years old which is justified by pathophysiology of OA. Matsumoto et al. performed a study in 2015 indicated that aging was associated with the lateral curvature of femoral shaft changing in the initiation of varus type OA of the knee. Following these changes, secondary signs of OA progression including varus femoral condylar orientation, medial joint space narrowing, and tibial plateau compression arise (22). Advancing age causes reductions in cartilage volume, proteoglycan content, cartilage vascularization, and cartilage perfusion and is the major risk factor for osteoarthritis in association with biochemical factors as mentioned by American Association of Orthopedic Surgeons (30).

Overcorrection and under correction of knee deformity lead to inconvenience and persistent pain in patient's knee (31). Accuracy in pre- and post-operative knee alignment radiography is an important factor that must be regarded. The gold standard modality for knee

Table 1. Comparison between single and double leg weight bearing radiography

Mean (degree)	Std. Deviation (degree)	Range (degree)	Paired Samples Test				
			Mean	Std. Deviation	Std. Error	Sig. (2-tailed)	
HKAA1	8.80	4.97	0.30-24.83	0.76	3.13	0.30	0.01
HKAA2	8.04	4.54	0.37-20.17				
MPTA1	89.25	5.71	76.80-103.37	0.36	6.97	0.67	0.59
MPTA2	88.89	9.32	19.50-102.43				
LDFA1	90.34	3.53	79.73-98.77	0.20	2.32	0.22	0.38
LDFA2	90.14	3.18	80.50-96.50				
JLCA1	3.44	2.64	0.00-15.83	0.42	1.82	0.18	0.02
JLCA2	3.02	2.38	0.07-11.63				

HKAA: Hip Knee Ankle Angle, MPTA: Medial Proximal Tibial Angle, LDFA: Lateral Distal Femoral Angle, JLCA: Joint Line Convergence Angle, 1: Stands for single leg, 2: stands for double leg weight-bearing

Table 2. Linear regression for time, observer, and position effects

	Variable	Level	Mean	SE	P
HKAA	Time	First Time	8.40	0.44	0.98
		Second Time	8.40	0.44	
	Observer	Observer 1	8.40	0.44	
		Observer 2	8.49	0.44	1.00
		Observer 3	8.37	0.44	
	Position	Standing on Single Leg	8.80	0.44	0.00
		Standing on Double Leg	7.99	0.44	
MPTA	Time	First Time	89.15	0.69	0.90
		Second Time	89.20	0.69	
	Observer	Observer 1	89.15	0.72	
		Observer 2	89.31	0.72	1.00
		Observer 3	88.75	0.72	
	Position	Standing on Single Leg	89.25	0.69	0.70
		Standing on Double Leg	89.11	0.69	
LDFA	Time	First Time	90.26	0.31	0.76
		Second Time	90.25	0.31	
	Observer	Observer 1	90.22	0.31	
		Observer 2	90.30	0.31	1.00
		Observer 3	90.19	0.31	
	Position	Standing on Single Leg	90.33	0.31	0.14
		Standing on Double Leg	90.14	0.31	
JLCA	Time	First Time	3.22	0.23	0.91
		Second Time	3.21	0.23	
	Observer	Observer 1	3.22	0.23	
		Observer 2	3.29	0.23	1.00
		Observer 3	3.19	0.23	
	Position	Standing on Single Leg	3.41	0.23	0.00
		Standing on Double Leg	3.02	0.23	

HKAA: Hip Knee Ankle Angle, MPTA: Medial Proximal Tibial Angle, LDFA: Lateral Distal Femoral Angle, JLCA: Joint Line Convergence Angle

alignment assessment is full limb lower extremity radiography in double leg weight bearing position. The current study was focused on full limb radiography and also compared double versus single leg weight-bearing positions. Van Raaij et al. in 2009 investigated two methods of femorotibial measurement on short knee images compared to the gold standard HKA angle on a full-limb view. Although angle on short knee images was correlated with HKA angle on full limb radiographs ($r=0.65$), these methods demonstrated poor inter- and intra-observer agreement ($ICC=0.37$) (14). Several studies were conducted for assessing reproducibility of angle measurements in short and full-limb radiographs. In 2009, Colebatch et al. compared and assessed the

reproducibility of knee axial alignment (HKA and FTA), on conventional AP knee and full-limb radiographs in healthy peoples. They suggested standard AP knee radiographs with proper reproducibility as a useful method for measuring knee alignment (18). But Sheehy et al. used the femoral shaft-tibial shaft angle (FS-TS) from short knee radiograph to estimate the HKA angle in OA patients. They recommended that use off full-length radiograph for an accurate estimation of HKA angle because FS-TS angle depends on direction and degree of knee deformity (27). In this study, four knee alignment parameters (HKAA, MPTA, LDFA, and JLCA) in both radiographs were assessed by three observers. The Results showed accurate inter-observer reproducibility

for all angles ($ICC>0.916$). Linear Regression results confirmed the reproducibility of the measurement by all three observers and indicated the independency of their experience ($P>0.05$). High intra-observer reproducibility was also obtained ($ICC>0.999$) and linear regression test confirmed the accuracy of time independency ($P>0.05$). These findings were consistent with the investigations of Matos et al. study. They evaluated inter and intra-observer analysis on measurements of the anatomical axis (FTA), as a fundamental element for assessing alignment of the lower limb, between AP full-limb and short film knee radiographs in OA patients. The results demonstrated that the methods for measuring the FTA on short and full limb radiographs were reliable and reproducible. In addition, observers experience had no impact on measurement results (13).

In the current study we demonstrated that HKAA and JLCA were significantly different between double and single leg weight-bearing positions. The linear regression analysis confirmed the effectiveness of the patient's position on these angles ($P=0.000$). According to Table 1. HKAA and JLCA were higher in single leg weight-bearing position which was similar to findings in the study of Specogna et al. They found that HKAA measured on single leg weight-bearing radiography is more representative of dynamic joint load and further highlights the difference between dynamic and static measures (24). During dynamic activities, such as gait, or single-leg weight-bearing, the force line shifts medial to the knee joint center, therefore the compressive stress is increased in medial aspect. Followed by this change the angles are higher while the patient is standing on single leg and varus deformity is augmented in this position (32).

The measurement of Knee alignment parameters (HKAA, MPTA, LDFA, and JLCA) on both radiographs by three observers indicated high inter-observer reproducibility for all angles and it was not affected by observer's experience. The results also showed high rate of intra-observer concordance and reproducibility. The present study found that HKA angle and JLC angle changed significantly in single leg versus double leg weight bearing position.

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The authors report no conflict of interest concerning the materials or methods used in this study or the findings specified in this paper.

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